



An excimer 'ON–OFF' switch based on telomeric G-quadruplex and rGO for trace thrombin detection

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ABSTRACT

In the recent decade, GO has emerged as an amazing 2D nanomaterial for developing DNA-based biosensors due to its fluorescence quenching properties, whereas similar research based on rGO was reported rarely. Herein, a novel multi-pyrene functionalized G-rich DNA probe based on the screened rGO showed much higher fluorescence quenching efficiency and excimer emission than that of universal GO. Different from the universal thrombin detection of the G4-forming aptamer-TBA(GGTGGTGTGGTGG), the original telomeric sequence is used in this study. The excimer emission "ON-OFF" switch amplified the response of thrombin detection is as low as 50 units. Furthermore, for four pyrene moieties that are sited in a crowded steric circumstance, the melting temperature (T_m) values and molecular dynamics simulations showed a positive effect on duplex G-quadruplex or c -DNA- c -DNA stability, without disturbing its helix structure.

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Since the first demonstration of a fluorescent probe based on graphene oxide (GO) complexed with single-stranded DNA (ssDNA) to bind complementary oligonucleotide sequences in 2009 [1], ssDNA/GO complexes, owing to their binding and quenching properties, have been widely applied to detect small molecules, metal ions, and biomolecules as well as for drug-delivery [2–5]. Generally, negatively charged ssDNA is adsorbed on the GO surface by ' π - π ' stacking between the DNA nucleobase moieties and GO carbon rings. Reduced graphene oxide (rGO) can be synthesized by the chemical reduction of GO, rGO possesses a high degree of aromaticity, which can facilitate a ' π - π ' stacking interface [6–9]. As a result, the different oxygen contents of rGO have various quenching efficiencies for the fluorescence intensity of labeled ssDNA and aptamers, even if the examples are deficient [10,11].

Furthermore, modified pyrene fluorophores exhibiting an emission excimer at red-shifted absorption are extensively being developed as desirable tools in diagnostics and nanomedicine [12]. Compared to various fluorophores, the excimer emission of pyrene derivatives is especially generated from a π -stack dimer between a pyrene unit in an electronically excited state and another in the ground state [13–15]. In 1996, the Kool group first reported the direct attachment of pyrene to deoxyribose, as pyrene is a chromophore replacing nucleobases [16]. Owing to dimer stacking

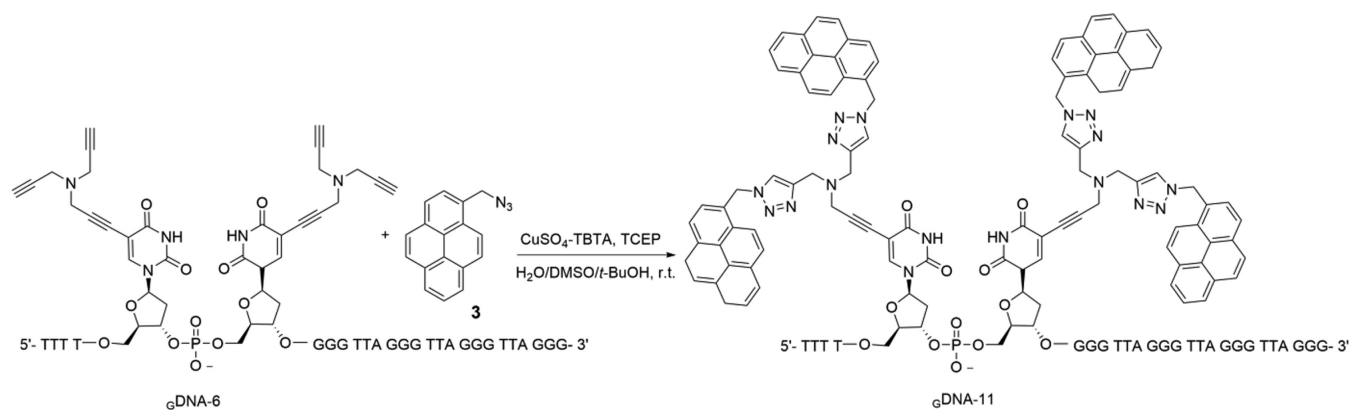
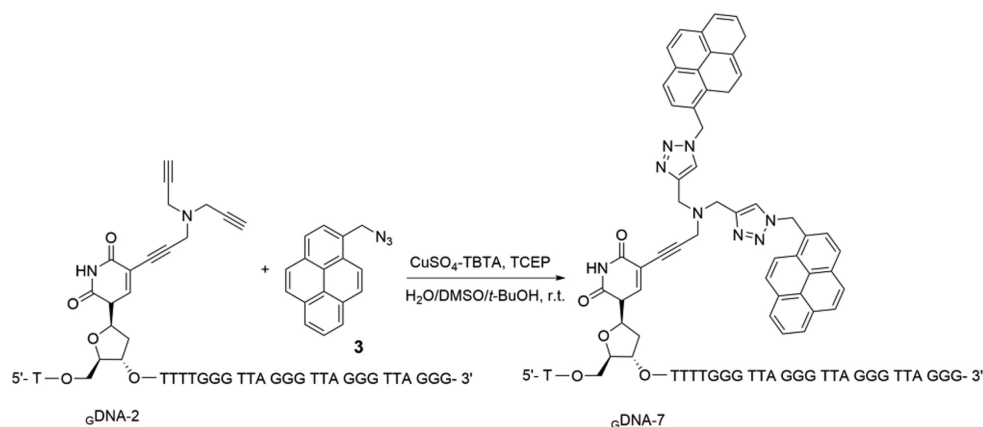
with a tremendous overlap in their π -orbitals, the earliest pyrene-containing multichromophores exhibit efficient excitation energy transfer and electron transfer [17,18]. To detect complementary DNA/RNA and the multi-labeling of RNA or LNA, more pyrene chromophores with non-nucleoside linkers have been incorporated into DNA in the last two decades [19–23].

G-quadruplexes are secondary structures of nucleic acids, which are composed of two or more stacked G-quartets with four guanine residues paired together through Hoogsteen-like hydrogen bonds. Endogenous G-quadruplex models have been confirmed in the promoter regions of numerous oncogenes and the human telomeric sequence, and they have been regarded as potential targets for anticancer drugs at the telomeric level with the inhibition of telomerase activity overexpressed in tumor cells [24–26]. Furthermore, the unique properties of G-quadruplexes have been investigated in some important reconstructions/reconfigurations and applications, including DNA origami, biosensing nanostructures, nanodevices, nanocarriers for disease therapeutics, and the detection of pathogens, including the causative agent of COVID-19 [27–32].

In 2012, Xiong *et al.* employed tripropargylated nucleosides to construct three-armed (Y-shaped) dendronized DNA *via* the 'stepwise and double click' approach [33]. In 2016, Kim and co-workers attached pyrene-modified monomers as dangling residues of the G-quadruplex. Red-shifted fluorescence emission was observed upon the addition of K^+ [34]. Herein, oligonucleotides containing single or multiple residues of tripropargylated 2'-

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Scheme 1. 'Click' reactions were performed on oligonucleotides and 1-azidomethylpyrene (**3**).

deoxyridine were prepared by the solid-phase synthesis of its phosphoramidites. Thereafter, the artificial ssDNA incorporating multi-pyrene moieties at the center or terminal sites could be obtained via the 'click' chemistry. Furthermore, the feasibility of using pyrene-functionalized G-rich human telomeric ssDNA as a fluorescence probe based on synthetic rGO was investigated. To optimize the sensitivity of the G-rich probe, the oxygen content of rGO was varied by analyzing the fluorescence quenching efficiency and excimer emission for multi-pyrene modification. Based on these results, various thrombin concentrations were detected.

According to previous studies, the 5-[di(prop-2-ynyl)amino]prop-1-ynyl derivative of 2'-deoxyuridine (**2**) was prepared from 5-iodo-2'-deoxyuridine (**1**) and 6-fold of tripropargylamine using the catalysts [Pd⁰(PPh₃)₄] and CuI. The Sonogashira cross-coupling reaction was performed to obtain nucleoside (**2**) in 71% yield. Further, the 'double click' reaction was carried out with nucleoside (**2**) containing two terminal triple bonds and 1-azidomethylpyrene (**3**) in the presence of CuSO₄ and sodium ascorbate (Scheme S1 in Supporting information). The corresponding phosphoramidite (**5**) was the final product, and all intermediates were characterized using ¹H and ¹³C NMR spectroscopy (Scheme S2 in Supporting information).

Modified oligonucleotides incorporating single or multiple residues of (**2**) were synthesized and constructed using standard solid-phase synthesis. The crude oligonucleotides were detritylated and purified by agarose gel electrophoresis or reversed-phase HPLC. To attach pyrene to the nucleobases on ssDNA, the 'double click' reaction was also performed on the nucleoside moiety (**2**) and 1-azidomethylpyrene (**3**) (Scheme 1). Oligonucleotides incor-

porating artificial residues (**4**) were confirmed by LC-ESI-TOF mass spectrometry (Table S1 and Fig. S1 in Supporting information).

The melting temperature (*T_m*) values of monomolecular G-quadruplexes or bimolecular duplexes incorporating single or multiple residues of (**4**) were measured by ultraviolet (UV) thermal denaturation (Figs. S2-S4 in Supporting information). *T_m* measurements showed that modifications with one or two moieties of (**4**), bearing oligonucleotides with two or four pyrene units, exhibited a positive effect on duplex or G-quadruplex stability. Indeed, an increase in *T_m* values for the unmodified oligonucleotides (*c*DNA-1 for G4 and *c*DNA-1·*c*DNA for duplex) is shown in Table 1. As a comparison, the attachment to oligonucleotides of single or multiple residues of (**2**) demonstrated a negative effect on duplex stability, with a decrease in the *T_m* values for the unmodified oligonucleotides (Table S2 in Supporting information). To determine whether *c*DNA formed G-quadruplexes in the PBS buffer (20 mmol/L, pH 7.0), *c*DNA-10 was chosen for CD analysis. The CD spectrum with a maximum band at approximately 264 nm and a minimum at approximately 241 nm indicated a quadruplex with all the strands oriented parallel to each other (Fig. S5 in Supporting information) [35–38].

Molecular dynamics simulations at the MM+ force field (HyperChem 8.0 Professional; Hypercube Inc.) were conducted on the 27-mer duplexes *c*DNA-6·*c*DNA, *c*DNA-8·*c*DNA, and *c*DNA-11·*c*DNA containing one or two modification sites in the duplex (Fig. 1). Fig. 1A shows a duplex containing two dU residues displaced by the nucleoside (**2**) residue at the proximal position. Molecular modeling indicates that the proximal nucleoside (**2**) moieties bearing terminal alkynes seem to interfere with the DNA helix and are

Table 1 T_m values of G-quadruplexes and pyrene oligonucleotide duplexes with mono- or multi-pyrene residues.

Pyrene modified duplexes	$T_m^{a,b}$ ($^{\circ}\text{C}$)	$\Delta T_m^{c,d}$ ($^{\circ}\text{C}$)
5'-d(TTT TTT GGG TTA GGG TTA GGG TTA GGG)-3' (c DNA-1) ^a 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC)-5' (c DNA)	50.5 ^a /65 ^b	
5'-d(T4T TTT GGG TTA GGG TTA GGG TTA GGG)-3' (c DNA-7) ^a 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC)-5' (c DNA)	57.5/67.5	+7 ^c /+2.5 ^d
5'-d(TTT TT4 GGG TTA GGG TTA GGG TTA GGG)-3' (c DNA-8) ^a 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC)-5' (c DNA)	51.5/65.5	+1/+0.5
5'-d(TTT TTT GGG 4TA GGG TTA GGG TTA GGG)-3' (c DNA-9) ^a 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC)-5' (c DNA)	51.5/66	+1.5/+1
5'-d(TTT TTT GGG TTA GGG 4TA GGG TTA GGG)-3' (c DNA-10) ^a 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC)-5' (c DNA)	51/67.5	+0.5/+2.5
5'-d(TTT T44 GGG TTA GGG TTA GGG TTA GGG)-3' (c DNA-11) ^a 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC)-5' (c DNA)	55/65	+4.5/+0

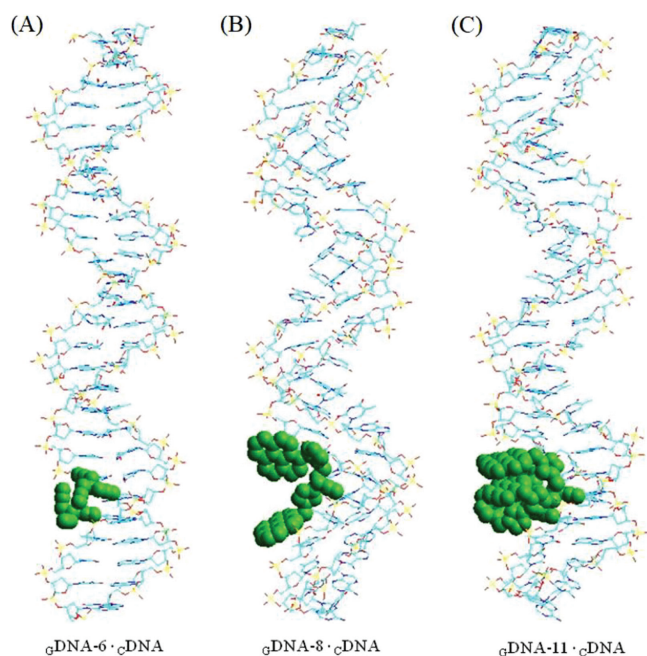
^a Measured at 295 nm in 20 mmol/L PBS buffer (pH 7.0) with 2 $\mu\text{mol/L}$ single-stranded concentration.^b Measured at 260 nm in 75 mmol/L Tris-HCl buffer (pH 7.5) with 2 $\mu\text{mol/L}$ + 2 $\mu\text{mol/L}$ single-stranded concentration.^c ΔT_m was calculated as $T_{m \text{ modified-quadruplex}} - T_{m \text{ unmodified-quadruplex}}$ using c DNA-1 as the reference unmodified quadruplex.^d ΔT_m was calculated as $T_{m \text{ modified duplex}} - T_{m \text{ unmodified duplex}}$ using c DNA-1/ c DNA as the reference unmodified quadruplex.

Fig. 1. Molecular models of (A) duplex 5'-d(TTT T22 GGG TTA GGG TTA GGG TTA GGG) (c DNA-6) · 3'-d(AAA CCC AAT CCC AAT CCC AAT CCC) (c DNA), (B) duplex 5'-d(TTT TT4 GGG TTA GGG TTA GGG TTA GGG) (c DNA-8) · 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC) (c DNA) and (C) duplex 5'-d(TTT T44 GGG TTA GGG TTA GGG TTA GGG) (c DNA-11) · 3'-d(AAA AAA CCC AAT CCC AAT CCC AAT CCC) (c DNA). The molecular dynamics models were simulated by using energy minimized AMBER calculations. The green balls are displayed as the modification sites.

not well adapted to the major groove. For the crowded steric situation, triazole rings of the modified derivative (**4**) at one or two proximal sites are not drawn while representing the stacking interactions of the nucleobase pairs (Figs. 1B and C). Molecular modeling indicated that despite the presence of four pyrene moieties in the crowded steric circumstance, all residues were well accommodated in the major groove without disturbing the DNA helix.

The oxygen contents of GO and rGO were measured by X-ray photoelectron spectroscopy (XPS). The GO samples showed characteristic peaks for carboxyl groups and C–O single bonds. After reduction by NaBH_4 (different reduction times), the oxygen content of rGO gradually decreased, as shown in Figs. S6 and S7 (Supporting information). rGO with different oxygen contents has different water solubilities. Indeed, rGO-5 and rGO-6 demonstrated poor dispersion in water. The size of GO and rGO on the mica flakes was confirmed by AFM. The thickness of GO and rGO is ap-

proximately 1.0 ± 0.2 nm. Considering the overestimation and the oxygen-containing group, the obtained thickness of approximately 1.0 nm for GO or rGO reasonably indicates a single-layer (Fig. S7B).

Owing to the different aromatic structures and oxygen content, GO and rGO have different adsorption capacities for ssDNA. In 20 mmol/L PBS buffer (pH 7.0), ssDNA was adsorbed on the GO or rGO surface in the form of a G-quadruplex. To investigate the fluorescence quenching efficiency, various concentrations of GO and rGO (0–50 $\mu\text{g/mL}$) were treated with c DNA-10 (Fig. S8 in Supporting information). Upon interaction with GO or rGO, the fluorescence intensity of c DNA-10 was substantially quenched. When 2 $\mu\text{g/mL}$ GO or rGO was added to the c DNA-10 in the PBS buffer, fluorescence quenching efficiencies of GO, rGO-1, rGO-3, and rGO-4 were below 20%. With a gradual increase in the GO or rGO concentration, the fluorescence intensity was further reduced. The rGO samples with a less oxygen content, rGO-5 and rGO-6, could not disperse well in water and aggregated rapidly, and therefore, they could not be used to investigate the interaction with c DNA-10.

Upon the addition of 30 $\mu\text{g/mL}$ rGO-2 in 1 $\mu\text{mol/L}$ solution of c DNA-10, the fluorescence intensity was quenched by 94% within 5 min, whereas the quenching of the fluorescence intensity of c DNA-10 (1 $\mu\text{mol/L}$) was approximately 84% by the addition of GO or other rGOs (Fig. 2A). Upon increasing the concentration of rGO-2 over 30 $\mu\text{g/mL}$, the fluorescence intensity of c DNA-10 (1 $\mu\text{mol/L}$) was quenched by more than 95% (Fig. 2B). When the concentration of rGO-2 was increased to 50 $\mu\text{g/mL}$, the fluorescence quenching efficiency of c DNA-10 reached 100%. The other rGO or GO samples did not show complete quenching even at higher concentrations (50 $\mu\text{g/mL}$). For comparison, the quenching efficiency of c DNA with different amounts of GO or rGO was also tested in 75 mmol/L Tris-HCl buffer at pH 7.5 (Figs. S9 and S10 in Supporting information). The optimized rGO-2 concentration of 30 $\mu\text{g/mL}$ was selected for fluorescence quenching with c DNA in subsequent assays.

A series of fluorescent quenching assays was performed on c DNA with different pyrene-labeled nucleoside positions after adding rGO-2 (30 $\mu\text{g/mL}$) (Fig. 2C). The fluorescence intensity of c DNAs (c DNA-7, c DNA-8, and c DNA-11) incorporating nucleoside (**4**) on the exterior of a G-quadruplex core was stronger than that of c DNAs containing the modified nucleosides inside the quadruplex region (c DNA-9 and c DNA-10). Usually, quenching effects are caused by guanine residues acting as the strongest quencher. When ssDNA forms a G-quadruplex structure in the PBS buffer, the pyrene moieties are rapidly involved in ' π - π stacking' with the G-tetrads, and the fluorescence intensity of c DNA with pyrene-modified nucleosides inside the G-quadruplex core decreases significantly. These findings are also in agreement with earlier observations of pyrene modifications in DNA duplexes [39–41]. GDNA-

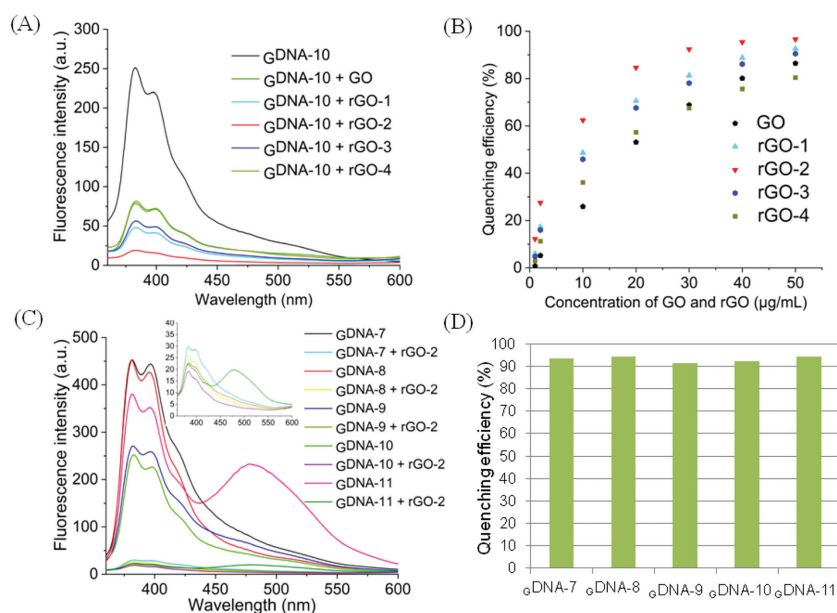


Fig. 2. (A) Fluorescence spectra of c DNA-10 before and after adding GO or rGO (30 μ g/mL) in PBS buffer (20 mmol/L, pH 7.0). (B) Fluorescence quenching efficiency (F_0-F)/ F_0 of c DNA-10 in terms of different concentrations of GO and rGO. F_0 and F are the fluorescence intensity before and after the addition of GO or rGO ($\lambda_{ex} = 340$ nm, c DNA-10 concentration = 1 μ mol/L). (C) Fluorescence spectra of c DNA before and after adding rGO-2 (30 μ g/mL) in PBS buffer (20 mmol/L, pH 7.0). (D) The fluorescence quenching efficiency (F_0-F)/ F_0 at 340 nm of λ_{ex} and concentration with 1 μ mol/L of c DNA.

11, incorporating two proximal derivatives, nucleoside **4** with four pyrene moieties in a crowded steric situation, triggered a red-shifted fluorescence excimer emission ($\lambda_{em} = 478$ nm). Upon the addition of 30 μ g/mL rGO-2, the fluorescence quenching efficiency of all c DNAs was more than 90% (Fig. 2D). The fluorescence quenching efficiency of different c DNA adsorbed on rGO-2 was also tested in 75 mmol/L Tris-HCl buffer (pH 7.5, Fig. S9). In the Tris-HCl buffer, the fluorescence intensity of c DNA-11 was 2-fold higher than that of GDNAs (from c DNA-7 to c DNA-10). As c DNAs assume a random-coil structure in the Tris-HCl buffer, the pyrene moieties cannot rapidly form the ' π - π stack' with the G-tetrads. These results showed that rGO-2 had a good quenching efficiency for c DNA in the Tris-HCl buffer.

Detecting the content of thrombin in tumor cells is of considerable significance for studying cancer cell proliferation and cancer diagnosis [42]. In 2010, Li *et al.* reported a graphene FRET aptasensor for thrombin detection. FAM aptamers are suitable for commercial use [43]. Using DNA intercalating dyes as FRET reporters, a quantum dot-aptamer beacon was successfully used for label-free thrombin detection [43]. Using a novel signal amplification strategy, Tang *et al.* developed a thrombin detection assay using a chiral supramolecular assembly with a physiological K^+ background in 2017 [44]. In contrast to the universal thrombin detection of the G4-forming aptamer-TBA(GGTTGGTGGTTGG), an original telomeric sequence was used in this study. Herein, we developed a new pyrene-labeled G-quadruplex and rGO-based biosensing platform for thrombin detection. The fluorescence recovery of the c DNA-11 and rGO-2 complexes is depicted upon the addition of different amounts of thrombin (Figs. 3A-C). Except for the fluorescence emissions at 381 nm and 395 nm, the excimer fluorescence at 478 nm also increased with the increasing concentration of thrombin. Compared with typical commercial dyes, these results can avoid the interference of many background signals for practical applications. The detection limit was 50 units of thrombin in a total volume of 1 mL. The addition of thrombin leads to fluorescence recovery owing to the formation of quadruplex-thrombin complexes, which have a weak affinity to rGO and push the dyes away from the rGO surface.

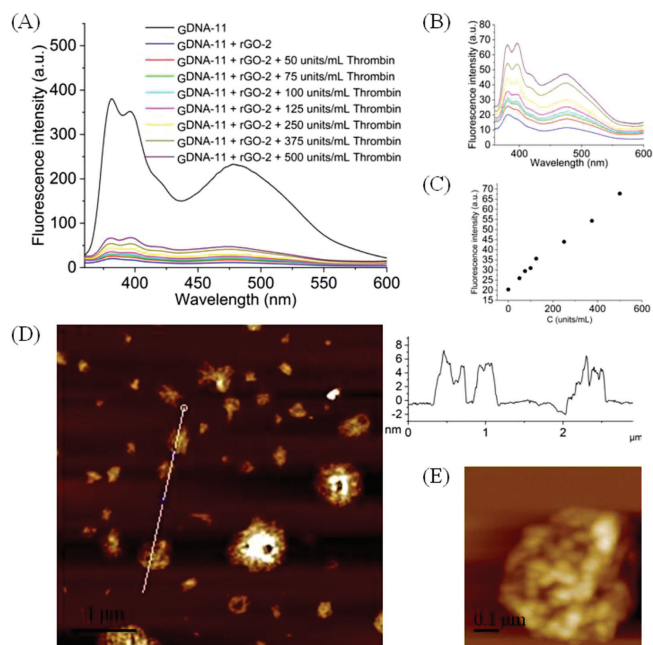


Fig. 3. (A) Fluorescence spectra of the c DNA-11 and rGO-2 via different concentrations of thrombin in 20 mmol/L of PBS buffer (pH 7.0, $\lambda_{ex} = 340$ nm, c DNA-11 concentration = 1 μ mol/L, rGO-2 concentration = 30 μ g/L). (B) The amplified fluorescence spectra of the c DNA-11 and rGO-2 after adding thrombin (from 0 to 500 units/mL). (C) Fluorescence intensity spectra of the c DNA-11 and rGO-2 after adding thrombin (from 0 to 500 units/mL, $\lambda_{ex} = 340$ nm, c DNA-11 concentration = 1 μ mol/L, rGO-2 concentration = 30 μ g/L). (D) AFM images including height profiles of c DNA-11 and rGO-2 sensor. (E) The amplified images of c DNA-11 and rGO-2 sensor. Scale size: 5 μ m \times 5 μ m.

Atomic force microscopy (AFM) was performed to observe the structure of the rGO- c DNA sensor. The typical images (Fig. 3D) displayed a few white areas on the rGO surface because of the presence of c DNA, with a thickness of less than 10 nm, for the rGO- c DNA biosensor. The c DNA sequences were uniformly dis-

tributed on the rGO surface without apparent selectivity, which is in good agreement with a previous report [45]. Besides, the details of $G_{\text{DNA-11}}$ are magnified and shown in Fig. 3E.

In this study, a series of mono- and multi-pyrene-labeled G-quadruplex sequences in different buffers were constructed. The ssDNA adsorbed on GO or rGO can be effectively protected against enzymatic degradation and biological interference *in vivo*. Furthermore, the adsorption of ssDNA on GO or rGO surfaces results in the exposition of ssDNA nucleic digestion and desorption of dsDNA, desorbed from the (r)GO by a complementary strand, to nuclease digestion *in vitro*. In the G-quadruplex form, the fluorescence intensity of multi-pyrene functional DNA probes decreases owing to the fluorescence quenching of stacked pyrene moieties, while T_m values show increased stability. Importantly, the G-quadruplex form with consecutive pyrene modifications ($G_{\text{DNA-11}}$) exhibited strong excimer emission. Further, the fluorescence quenching of DNA based on GO and rGO with different oxygen contents was investigated in PBS or Tris-HCl buffers. Furthermore, the morphology of the rGO-based aptasensor assembled with the pyrene-labeled G_{DNA} was determined by AFM.

In this study, negatively charged rGO demonstrated a better fluorescence quenching efficiency for DNA aptamer compared to GO. As an optimized result, the G-quadruplex form with consecutive pyrene modifications ($G_{\text{DNA-11}}$) based on rGO-2 was selected as a biosensor to detect thrombin. Moreover, the application of such kind of optical or electrical G-quadruplex rGO-biosensor in cancer cell recognition will open the possibility of diagnostics and other diverse nano-medical applications.

Declaration of competing interest

The authors declare no conflict of interest.

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Supplementary materials

Supplementary material associated with this article can be found, in the online version, at doi:10.1016/j.ccl.2022.02.048.

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